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### **P6.19: EFFECTS OF CARDIAC MOTION ON THE LEFT CORONARY ARTERY FLOW RATE**

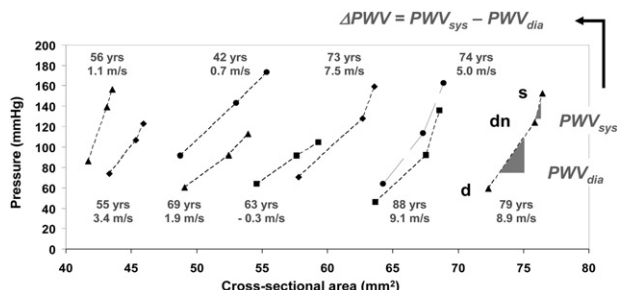
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**Methods and Results:** In 29 patients (21m/8f), carotid artery blood pressure and CSA waveforms were obtained by catheter and ultrasound. Diastolic, systolic and diastolic notch amplitudes were determined for each individual (Figure). In 15 older patients (77±5yrs) compared to 14 younger (59±7yrs) carotid  $\Delta$ PWV and CSA were increased (+2.6m/s and +7mm<sup>2</sup>, resp.,  $p < 0.03$ ), despite similar blood pressures. Moreover, in multiple regression analyses, age was a determinant of both  $\Delta$ PWV and CSA, independent of sex, height and pulse pressure ( $p < 0.01$ ).



Older patients have a more non-linear pressure-area curve, at a greater cross-sectional area. Tags shows age and  $\Delta$ PWV of the subjects. S denotes systolic; d, diastolic; dn, diastolic notch. (Only a sample of 29 is shown for clarity.) PWV values are calculating using Bramwell-Hill:  $PWV = \sqrt{1/\rho \cdot \text{distensibility}}$ .

**Conclusions:** Our study demonstrates detectable age-related differences in carotid stiffness non-linearity and cross-sectional area, suggesting these may act as markers of vascular ageing.

#### P6.18

##### COMPARISON OF ARTERIAL STIFFNESS ASSESSED BY ARTERIOGRAPH WITH ARTERIAL STIFFNESS ASSESSED BY APPLANATION TONOMETRY AND ECHOTRACKING: A CLINICAL STUDY

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**Introduction:** Large artery stiffness is recognized as a strong, independent marker of cardiovascular risk, mainly through aortic pulse wave velocity (PWV). Arteriograph is a new non-invasive oscillometric method, which estimates aortic PWV through brachial pressure wave analysis. In a previous study, Trachet et al. (*Annals of Biomedical Engineering* 2010) have shown, using a numerical model of arterial tree, that Arteriograph measured a brachial stiffness instead of aortic stiffness.

**Aim:** To compare PWV with Arteriograph (Ar PWV) to carotid-femoral PWV (CF PWV), carotid-radial PWV (CR PWV) and carotid-humeral PWV (CH PWV). And to compare Ar PWV to carotid stiffness (CS) and humeral stiffness (HS).

**Methods:** CF, CH, and CR PWV were assessed by applanation tonometry (SphygmoCor®). Ar PWV was assessed by Arteriograph and CS, HS were assessed by echotracking system (Mylab®). Pearson's correlation coefficient,  $r$ , between the methods was calculated.

**Results:** 43 subjects were included: 20 healthy subjects and 23 patients with essential hypertension. The correlation between CF PWV and Ar PWV is good and significant in healthy subjects and all subjects ( $r = 0.77$  and  $r = 0.76$  respectively  $p < 0.001$ ), and weak but not significant in hypertensive subjects. The same with CS in all subjects only ( $r = 0.72$ ,  $p < 0.001$ ) There are no significant correlation between Ar PWV and CH PWV, CR PWV, HS.

**Conclusion:** Arteriograph is well correlated with CF PWV and CS in all subjects but not with brachial stiffness. Nevertheless, it is necessary to include more subjects in this study to see if the correlation is as well in healthy subjects and hypertensive patients.

#### P6.19

##### EFFECTS OF CARDIAC MOTION ON THE LEFT CORONARY ARTERY FLOW RATE

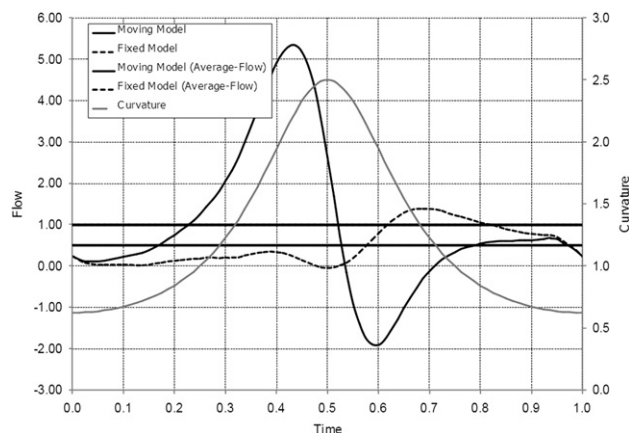
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The aim of this work was to investigate the effects of physiologically idealized cardiac-induced motion on flow rate in human left coronary arteries. The blood flow rate were numerically simulated in a elastic

modelled left anterior descending coronary artery (LAD) having a uniform circular cross section of 3.6 mm diam. Blood was considered to be a non-Newtonian fluid and Arterial motion was specified based on monoplane physiologically idealized bending. Simulations were carried out with dynamic pressure difference conditions between inlet and outlet in both fixed and moving LAD models, to evaluate the relative importance of LAD motion, flow rate, and the interaction between motion and time-averaged flow rate. LAD motion was caused variations in time-averaged flow rate magnitude about 30% of the fixed models. There was significant variability in the magnitude of this motion-induced flow variation. However, the magnification of time-averaged flow rate is depending to specification of the cardiac motion. Furthermore, the effects of pressure pulsatility dominated LAD motion induced effects; specifically, there were local flow variation and secondary flow in the simulations conducted in moving LAD models. LAD motion has big effect on time-averaged flow rate and secondary flow. Therefore, the hemodynamic effects of LAD motion can not be ignored as a first approximation in modelling studies.



**Figure 1** Temporal and time-averaged flow at 11 diameters distance from the LAD inlet for both moving and fixed models.

#### P6.20

##### VASCULAR ACCESSES FOR HAEMODIALYSIS IN THE ARM CAUSE GREATER REDUCTION IN THE CAROTID-BRACHIAL STIFFNESS THAN THOSE IN THE FOREARM: STUDY OF GENDER DIFFERENCES

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**Purpose:** to evaluate in chronically-haemodialysed patients (CHP) if, 1) the vascular access (VA) position (arm or forearm) is associated with differential changes in upper-limb arterial stiffness; 2) differences in arterial stiffness exist between genders associated with the VA; 3) the vascular substitute (VS) of choice, in biomechanical terms, depends on the previous VA location and CHP gender.

**Methods:** Clinical and biochemical parameters and left and right carotid-brachial pulse wave velocity (PWVcb) were measured in 38 CHP (males:18; Age:53±17 years; VA in arm:18). In *in vitro* studies, PWV was obtained from ePTFE prostheses and human arterial and venous homografts (brachial, femoral and carotid arteries and saphenous veins). The biomechanical mismatch (BM) between CHP native vessel (NV) and VS was calculated.

**Results:** PWVcb in upper-limbs with VA was lower than in the intact contralateral limbs, and differences were higher ( $P < 0.02$ ) when the VA was performed in the arm. Differences between PWVcb in upper limbs with VA (in the arm) with respect to intact upper-limbs were higher ( $P < 0.01$ ) in males than in females. Independently of the arterial region in which the VA was performed, the type of homograft that ensured the minimal BM was the brachial artery. The BM between VS and NV was highly dependent on gender and the location in the upper-limb in which the VA was performed.