

# An Algorithm for the Evaluation of the Dynamics of Blood Flow in the Carotid Arteries and the Air Flow in the Trachea of the Resuscitated Patient

Artem Sh. Bureev, Dmitry S. Zhdanov, Ekaterina Yu. Kiseleva, Mikhail S. Kutsov  
National Research Tomsk State University  
Tomsk, Russia  
eka.kiselyova@gmail.com

**Abstract** – The article is to study evaluation algorithms of the dynamics of blood flow and air flow recorded in the bifurcation area of the carotid artery and trachea, underlying in the operation of the device for the control of cardiopulmonary resuscitation procedure of a human.

**Keywords** - cardiopulmonary resuscitation, evaluation of blood flow dynamics, assessment of breathing dynamics, carotid bifurcation, trachea, analysis acoustic signal.

## I. INTRODUCTION

Sudden cardiac death is the leading cause of death in the world. Thus, in the US, the number of sudden cardiac death is 1 case per 1000 people per year, while in Russia - up to 2 cases per 1000 people. Emergency assistance for people with cardiac failure - sudden cardiac death - remains an urgent problem not only in emergency medicine, but also in therapy and cardiology in particular [1, 2, 3].

According to the statistical data, up to 90% of the patients who faced clinical death could survive, if they received adequate medical care within the first 5 minutes after cardiac arrest. Unfortunately, even at large medical institutions, physicians often cannot perform the cardiopulmonary resuscitation (CPR) procedure in compliance with recommendations.

Mortality reducing is an important task of providing emergency medical care. According to [4], most people do not have sufficient skills in cardiopulmonary resuscitation. Therefore, devices allowing a person, performing the procedure of cardiopulmonary resuscitation (hereinafter - CPR), to obtain feedback about the correctness of the procedure, are in high demand.

Currently in the market there are no mobile devices for non-stop real-time evaluation of the adequacy of resuscitation and for the control of the patient's state during and after the procedure.

The design team of the Professional Equipment Engineering Research Laboratory of National Research Tomsk State University are working on the development of an experimental sample of the device for the control of CPR (hereinafter - the device [5]). The device is aimed at analysis of

acoustic blood flow signals and air flow recorded in bifurcation area of the carotid artery and trachea for evaluating the correctness and adjustment of the actions of the personnel conducting CPR.

The operating mode of the device is determined by availability of the vital functions of the patient:

- *Monitoring* mode: cyclical check of vital functions of the patient;
- *Resuscitation* mode: evaluating the correctness and adjustment of the actions of the resuscitator.

Implementation of the above-described principle requires complex software algorithms for assessment of the dynamics of blood flow in the carotid arteries and air flow in the throat of the resuscitated patient by means of analyzing acoustic signals. The algorithms allow detecting the presence of vital functions in case of a positive effect of the resuscitation. Operation of the device in *Monitoring* mode allows a resuscitator to determine the time of a subsequent cardiac arrest urgently. The vital functions of a patient in *Monitoring* mode are determined during the assessment of the blood flow in the bifurcation area of the carotid artery and air flow in the patient's trachea.

## II. ASSESSMENT ALGORITHM OF THE DYNAMICS OF BLOOD FLOW IN THE CAROTID ARTERIES

Currently only Doppler-based ultrasonic angiography is used for determination of the blood flow dynamics. However, the use of the Doppler Effect for determination of the true blood flow speed (dynamics) in the carotid arteries will complicate the design of the sensor due to the required angle between the ultrasound transducer and the patient's neck.

In addition, application of an ultrasonic transmitter and receiver is not possible without immersion liquid necessary to avoid ultrasonic attenuation which is unacceptable during the resuscitation as it may require extra time for fixing the sensors on the patient's neck. Thus, the design team found a piezoelectric transducer the most suitable for receiving acoustic signals from the patient's neck.

As the device evaluates the acoustic blood flow signal, its dynamics can be evaluated with a blood beat number in the area of division of the carotid arteries for a certain period of time.

In *Monitoring* mode evaluation algorithm for noise recorded in the bifurcation of the carotid artery is applied. Blood flow dynamics can be taken as a binary function that can be valued as:

- 0 if there is no heart;
- 1 if there is a heartbeat.

Figure 1 shows a graphic of the function describing the dynamics of the blood flow in the carotids.

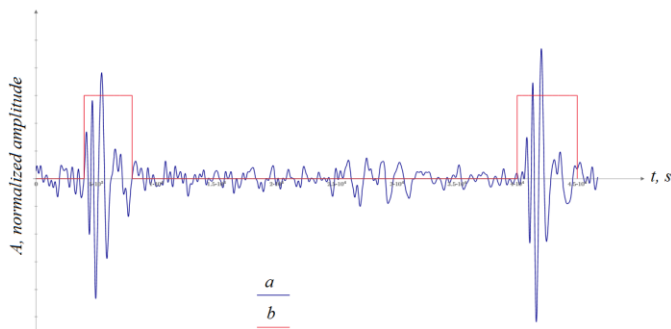


Fig. 1. Function describing the dynamics of the blood flow in the carotids. (a - acoustic signal recorded in the bifurcation area of the carotid arteries; b - a binary function showing the blood flow dynamics.)

After a positive effect of the resuscitation a patient may have bradycardia (heart rate about 25-60 beats per minute).

Thus the minimum number of blood flow beats, registered by acoustic sensors in the bifurcation area of the carotid arteries, will be 12.

Within 30 seconds, in *Monitoring* mode the number of blood beats in the area of carotid bifurcation is counted.

Figure 2 shows the basic block diagram of the algorithm for estimating the dynamics of air flow in the trachea.

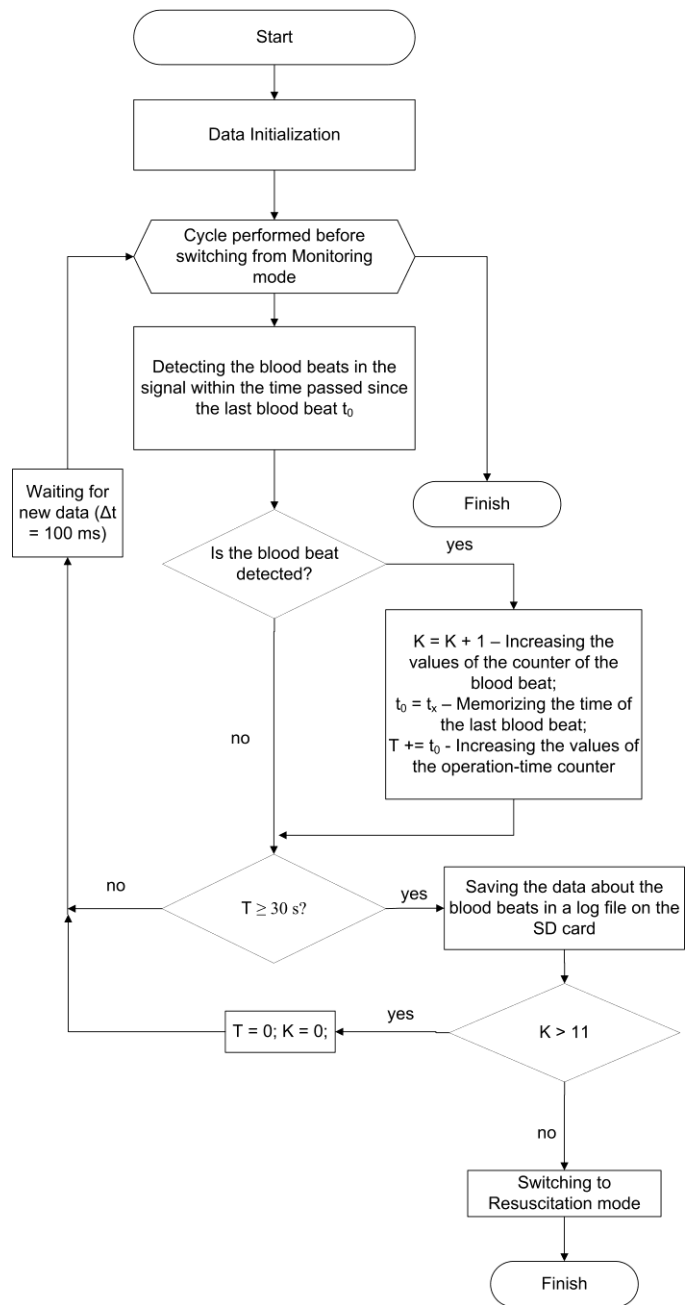


Fig. 2. The basic block diagram of the algorithm for estimating the dynamics of air flow in the trachea.

The algorithm of blood flow dynamics evaluation in the area of carotid bifurcation is performed continuously in the *Monitoring* mode and starts immediately when the device is in this mode. The sequence of cyclical actions:

- 1) to prepare variables, reset to 0 their values;
- 2) to perform a sequence of actions when device is turned on and is in *Monitoring* mode:
  - a) to determine the presence of blood beats in the area of carotid bifurcation in the signal section from  $t_0$  to  $t_x$ , where  $t_0$  - time of the end of the last blood beat found,  $t_x$  - the current time of the end of the signal;
  - b) If the blood beat is not detected, go to step d;

- c) if blood beat is detected, memorize the new time of the end of the last beat found  $t_0$ ,  $F$ , increase blood counter;
- d) If the operation time  $T$  of the cycle is less than 30 seconds, go to step 3;
- e) If the operation time  $T$  of the cycle is more or equal to 30 seconds, save the current data about the blood flow in a log file on the SD card;
- f) if the number of blood beats in the area of carotid bifurcation  $K$  is more than zero, reset variables of the cycle time  $T$  to 0 and the number of blood beats  $K$ , go to step 3;
- g) if the number of blood beats  $K$  equals zero, put the device in *Resuscitation* mode and complete the operation work cycle;

3) wait for the new acoustic data of the blood flow for a while and continue performing from step 2.

The basic block diagram of the algorithm for estimating the dynamics of air flow in the trachea is shown in Figure 2.

Thus, as soon as the device detects a patient's heart rate lower than 24 beats per second, a sound signal alarms a resuscitator about the possible need to start the resuscitation procedure.

### III. ALGORITHM FOR ESTIMATING THE DYNAMICS OF AIR FLOW IN THE TRACHEA OF THE RESUSCITATED PATIENT

At the moment for the registration of the breathing characteristics, including air flow rate, spirometry and plethysmography are generally used.

Spirometry is a graphic registration of changes in lung volume during respiration. Plethysmography allows measuring volume of thoracic gas, calculating airway resistance of the respiratory tract and estimating the shape of the resistance curve [6, 7].

However, these methods can not be used in the device for controlling the CPR procedures as they need additional devices for data processing. It certainly leads to an increase of time of preparation, which is unacceptable in the critical situation of saving of a human life.

The most suitable method for assessing the dynamics of air flow in the trachea in terms of reliability and technical feasibility is the method of analysis of the acoustic signals received from the surface between the presternum and shield-like cartilage on the trachea of the resuscitated patient.

It can be assumed that the air flow dynamics in the trachea is presence or absence of air flow in the trachea for 30 seconds.

According to the functioning algorithm of the Device, evaluation of air flow speed [5] in the trachea of the resuscitated patient is performed in *Monitoring* mode in the survey of acoustic sensors every 30 seconds.

Thus, the dynamics of air flow in the trachea is considered in terms of number breaths within 30 seconds.

A healthy adult in a state of physiological dormancy averagely performs 16 to 20 breaths per minute. In the dream, breathing slows down to 12-14 breaths per minute, and during physical activity, emotional excitement or after eating it naturally quickens [8].

In case of a positive response of the patient to the CPR respiratory rate acceleration (tachypnea) or respiratory rate deceleration (bradypnea) can occur.

In case of tachypnea respiratory rate reaches more than 20 breathing cycles per 1 minute for an adult. In case of bradypnea respiratory rate reaches 10-12 or even fewer breathing cycles per 1 minute.

In case of bradypnea after the resuscitation, within 30 seconds (in the worst case scenario) only one respiratory cycle can be found.

Figure 3 shows a real acoustic respiration signal. Thus, the dynamics of air flow in the trachea can be taken as a binary function, which equals 1 in the presence of acoustic breath sounds and 0 in their absence. The signal of dynamics is shown in Figure 3 (curve - 1).

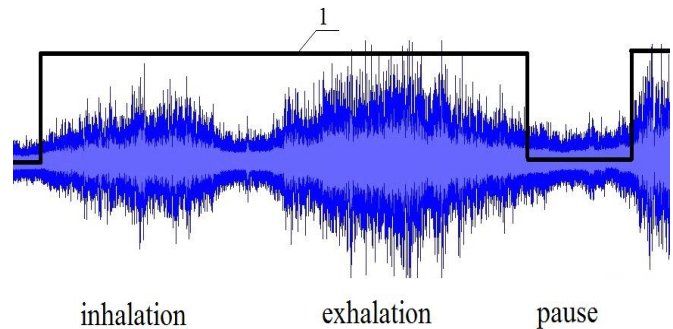


Fig. 3. The acoustic signal of respiratory noise (1 – The function of the dynamics of air flow in the trachea).

Thus, the algorithm of dynamics estimation of air flow in the trachea aims at calculation of the respiratory sounds within 30 seconds (Figure 7). If during those 30 seconds there are no respiratory noise signal found, the Device enters *Resuscitation* mode. In other cases, the Device operates in *Monitoring* mode.

The algorithm of dynamics estimation of air flow in the trachea (Figure 4) is applied during the entire time of the device operating in *Monitoring* mode and starts immediately when the device is in this mode. The sequence of cyclical actions:

- 1) to prepare variables, reset to 0 their values;
- 2) to perform a sequence of actions when device is turned on and is in *Monitoring* mode:
  - a) to determine the presence of respiratory movements in the area of the signal from  $t_0$  to  $t_x$ , where  $t_0$  - time of the end of the last respiratory movement found,  $t_x$  - the current time of the end of the signal;
  - b) if the respiratory movement is not detected, go to step d);
  - c) if a respiratory movement is detected, memorize the new time of the end of the last respiratory movement found  $t_0$ , increase the operation-time counter, increase respiratory movements counter;
  - d) If the operation time  $T$  of the cycle is less than 30 seconds, go to step 3;
  - e) If the operation time  $T$  of the cycle is more or equal to 30 seconds, save the current data about the breathing in a log file on the SD card;

f) if the number of respiratory movements  $D$  is more than 0, reset to 0 cycle time variables  $T$  and number of breaths  $D$ , go to step 3;

g) if the number of respiratory movements  $D$  equals 0, switch to a *Resuscitation* mode and complete the cycle operating;

3) wait for a while for the new acoustic respiration data and continue from step 2.

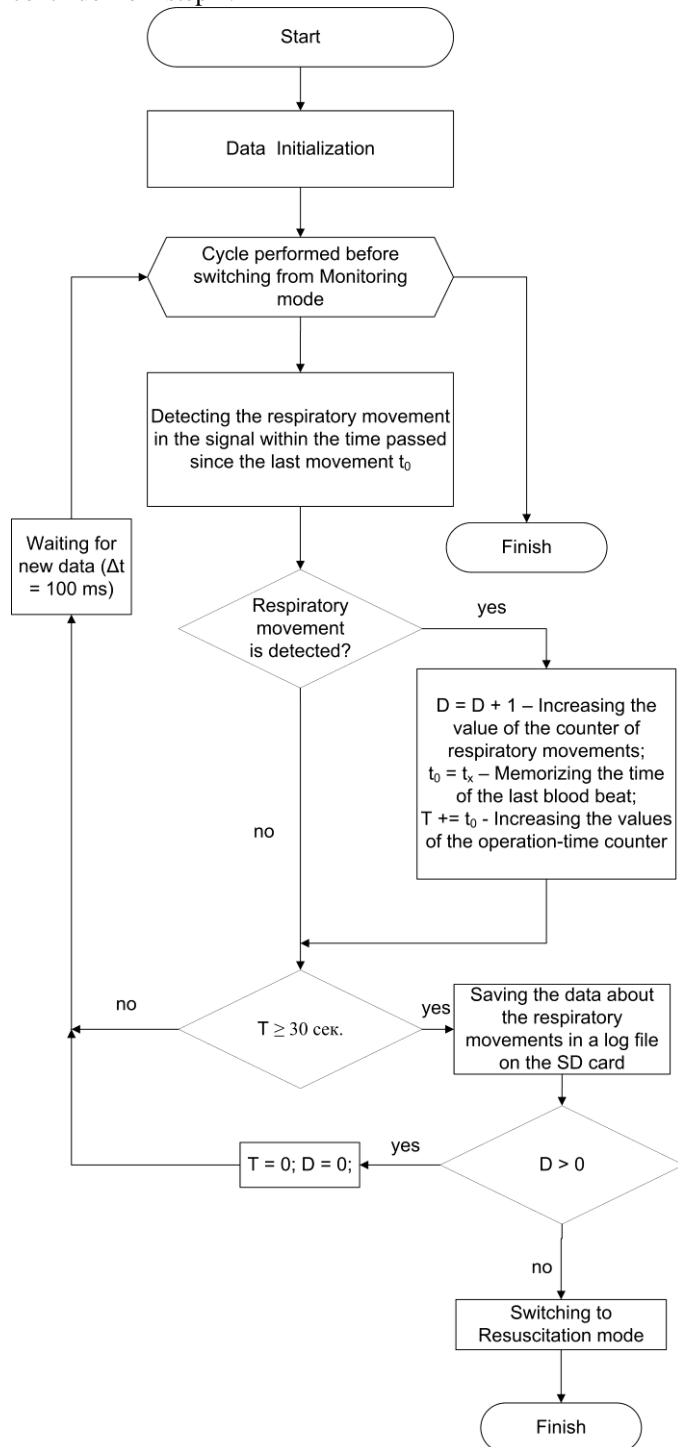


Fig. 4. The basic block diagram of the algorithm for estimating the dynamics of air flow in the trachea.

#### IV. CONCLUSION

The result of the work presents a developed set of software algorithms for assessment of the dynamics of blood flow in the carotid arteries and air flow in the larynx of the resuscitated patient with the aid of acoustic signals analyzing.

The software runs as part of the device for the control of the CPR procedure of a human.

These algorithms developed operate simultaneously and allow resuscitators to detect the subsequent cardiac and respiratory arrest urgently. This will allow to start resuscitation procedure in time and improve the survival rate by reducing the reaction time of the resuscitator at the time of the subsequent clinical death.

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